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Osteogenic index of step exercise depending on choreographic movements, session duration, and stepping rate

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Background: Step exercise has been promoted as a low impact physical activity recommended for the improvement of cardiorespiratory and muscular fitness. This recreational activity might also be recommended to improve bone health since mechanical load plays an important role in the normal development of the skeleton.

Methods: Our main purpose was to characterise 100 step sessions and to calculated osteogenic index (OI) according to Turner and Robling: OI (one session)= peak ground reaction force (BW)×ln (number of loading cycles+1).

Results: Main results (mean±SD) were as follows: OI was 12.0±0.8; peak ground reaction force (GRF) was 1.40±0.10 times body weight (BW); session duration was 38.6±8.3 min; stepping rate was 134.6±4.7 beats per minute (bpm); the movements performed most often were marching, knee hop, side leg, L step, and over the top; and the number of loading cycles was 4194.1±1055.2. OI and GRF increased significantly when stepping rate was higher than 135 bpm. This stepping rate might be used as a reference for higher intensity classes. A frequency of two to three sessions per week of step exercise is recommended.

Conclusions: Despite the benefits that have been stated when step classes are structured correctly and adapted to the participants, further research is needed concerning biomechanical load, exercise prescription, and injury prevention.

Step exercise has been promoted as a low impact physical activity recommended for the improvement of cardiorespiratory and muscular fitness. The main goals of performing step-on (forward-ascending) and step-off (backward-descending) movements combined with marching, dancing, jogging, and jumping exercises, as part of choreographed sequences using a step bench 10–25 cm high, are to obtain metabolic and mechanical benefits for health and fitness. Step movements use right or left leading legs, single or alternate leading steps, and propulsion or non-propulsion steps. Different choreographic patterns determine exercise intensity. Care must be taken in relation to the different movements chosen by instructors in each session and the mechanical load selected to provide a safe and effective exercise program. Previous studies have shown that biomechanical intensity is related to bench height and stepping rate. 3–5 The osteogenic potential of physical activity can be improved by correctly structuring exercise sessions and defining the rate and magnitude of skeletal loading. External loads produce internal forces which constitute the mechanical load which is related to the osteogenic potential of physical activity. On the other hand, mechanical load may also be implicated in musculoskeletal injuries to the knee and ankle. Our major concern is how to best exercise while maintaining safe levels of mechanical load. The characterisation of stepping exercise requires the study of a large variety of movements with different motor patterns.

It is widely accepted that physical exercise increases and maintains bone mass and strengthens bone. Also, vigorous exercise during growth and young adulthood may well reduce fracture risk in later decades. 4–5 However, there is no clear consensus on the best exercises and how often one should exercise. During exercise ground reaction forces (GRF) and internal forces are imposed on the skeleton. It is thought that bones respond to the strains imposed by these forces. Dynamic and high magnitude loading elicits a greater strain rate in bones and is known to be effective for anabolic loading. 4 These forces are created during movement by muscle contractions and by impact with external objects, such as the ground in walking. 4 It has been reported that mechanical loading generated by physical activity levels leads to improvements in skeletal development, mainly because weight bearing during exercise plays an important role in improving the mechanical properties of bone. 4 When new forces or loads alter the normal daily pattern of bone bending and strain, the bone adapts by increasing formation that in turn increases mass, size, and moment of inertia to resist the altered bending. 4 Huang et al 6–10 concluded that different modes of exercise may benefit bone mechanical properties in different ways. Turner and Robling 4 reported that load induced bone formation was improved by periods of rest. They also reported that as these no-loading periods were lengthened, bone formation was further enhanced, and after 24 h of rest, 98% of bone mechanosensitivity was restored. Consequently, the osteogenic response to exercise can be enhanced by regimens that incorporate periods of rest between short vigorous skeletal loading sessions. Prolonged loading repetitions can diminish the mechanosensitivity of bones, but increased intervals between loading might restore sensitivity. 4 Turner and Robling 4 demonstrated that the osteogenic potential of exercise was improved by increasing the rate and magnitude of skeletal loading and separating exercise into many short sessions. These authors developed a new measure of effectiveness for exercise protocols called the osteogenic index (OI) which depends on the exercise intensity (peak GRF) and desensitisation, allowing the estimation of bone formation. For instance, the weekly OI

Abbreviations: BW, body weight; GRF, ground reaction force; OI, osteogenic index
Table 1: Maximal vertical ground reaction force in normalised body weight of 15 experienced subjects

<table>
<thead>
<tr>
<th>Pattern</th>
<th>Mean GRF (BW) at 130 bpm</th>
<th>Mean GRF (BW) at 140 bpm</th>
<th>Loading cycles</th>
<th>Motor pattern</th>
</tr>
</thead>
<tbody>
<tr>
<td>Basic step</td>
<td>1.46 ± 0.30</td>
<td>1.54 ± 0.34</td>
<td>2 for ascending and 2 for descending</td>
<td>Pattern 1: step on/step on/step off/step off</td>
</tr>
<tr>
<td>Knee lift step</td>
<td>1.50 ± 0.17</td>
<td>1.55 ± 0.23</td>
<td>1 for ascending and 2 for descending</td>
<td>Pattern 2: step on/knee lift/step off/step off</td>
</tr>
<tr>
<td>Knee triple repeater</td>
<td>1.60 ± 0.22</td>
<td>1.69 ± 0.24</td>
<td>2 with propulsion for propulsion</td>
<td>Pattern 3: step on/triple knee lift repeater/step off/step off</td>
</tr>
<tr>
<td>Run step</td>
<td>2.09 ± 0.25</td>
<td>2.17 ± 0.27</td>
<td>2 for descending</td>
<td>Pattern 4: jump on/jump off/step off/step off</td>
</tr>
<tr>
<td>Knee hop step</td>
<td>1.74 ± 0.16</td>
<td>1.76 ± 0.19</td>
<td>2 for ascending (1 with propulsion) and 2 for descending</td>
<td>Pattern 5: step on/hop knee lift/step off/step off</td>
</tr>
</tbody>
</table>

Values are mean ± standard deviation for seven step movements performed at 130 and 140 bpm using a 15 cm bench, and respective numbers of loading cycles and motor pattern. GRF for marching and running are also presented. BW, body weight; GRF, ground reaction force.

Table 2: Statistical analysis of 100 step exercise classes

<table>
<thead>
<tr>
<th>Duration (min)</th>
<th>Minimum stepping rate (bpm)</th>
<th>Maximal stepping rate (bpm)</th>
<th>Mean stepping rate (bpm)</th>
<th>Loading cycles (n)</th>
<th>Step movements (n)</th>
<th>Non-propulsion movements (%)</th>
<th>Propulsion movements (%)</th>
<th>Peak GRF (BW)</th>
<th>Osteogenic index</th>
</tr>
</thead>
<tbody>
<tr>
<td>Median</td>
<td>38</td>
<td>130</td>
<td>138</td>
<td>135.4</td>
<td>41.44</td>
<td>1392</td>
<td>80</td>
<td>20</td>
<td>1.42</td>
</tr>
<tr>
<td>Min</td>
<td>25</td>
<td>120</td>
<td>128</td>
<td>124.9</td>
<td>187.4</td>
<td>624</td>
<td>48</td>
<td>0</td>
<td>1.26</td>
</tr>
<tr>
<td>Max</td>
<td>58</td>
<td>142</td>
<td>150</td>
<td>144.7</td>
<td>725.0</td>
<td>2524</td>
<td>100</td>
<td>52</td>
<td>1.16</td>
</tr>
<tr>
<td>Range</td>
<td>33</td>
<td>22</td>
<td>22</td>
<td>19.8</td>
<td>5376</td>
<td>1900</td>
<td>52</td>
<td>52</td>
<td>0.39</td>
</tr>
<tr>
<td>Mean</td>
<td>38.6</td>
<td>130.6</td>
<td>138.3</td>
<td>134.6</td>
<td>419.41</td>
<td>1422.6</td>
<td>79.4</td>
<td>20.6</td>
<td>1.40</td>
</tr>
<tr>
<td>SD</td>
<td>8.3</td>
<td>5</td>
<td>4.4</td>
<td>4.7</td>
<td>1055.2</td>
<td>384.5</td>
<td>10.5</td>
<td>10.5</td>
<td>0.10</td>
</tr>
</tbody>
</table>
pressure insoles with 99 sensors (table 1). Using the total number of step movements, a weighted average of the peak GRF of the session was determined using Excel as shown in eqs 1 and 2 (which were derived from table 1). The total number of step movements and the movements performed most often were recorded. Also, the percentage of non-propulsion/propulsion movements was determined. The osteogenic index was calculated in Excel using the equation of Turner and Robling: $\text{OI(1 session/day)} = \text{peak GRF(BW)} \times \ln(\text{loading cycles} + 1)$.4

\[
\text{eq 1}
\]

\[
\text{GRF of the step class at 130 bpm} = \\
\text{Number of cycles of movements with pattern 1 x 1.49 BW} + \\
\text{Number of cycles of movements with pattern 2 x 1.50 BW} + \\
\text{Number of cycles of movements with pattern 3 x 1.60 BW} + \\
\text{Number of cycles of movements with pattern 4 x 2.09 BW} + \\
\text{Number of cycles of movements with pattern 5 x 1.74 BW} + \\
\text{Number of cycles of movements with pattern "March" x 1.06 BW} + \\
\text{Number of cycles of movements with pattern "lunge" x 1.30 BW}
\]

\[
\text{Total number of loading cycles}
\]

Median, minimal, maximal, range, mean, and standard deviation values for total session duration (min), minimum, maximal, and mean stepping rate used in sessions (bpm), number of loading cycles, number of step movements, percentage of non-propulsion/propulsion movements observed in 100 sessions, as well as weighted peak GRF normalised in BW and osteogenic index were calculated. Kolmogorov-Smirnov normality tests, one way ANOVA, and Tukey post hoc test were performed using SPSS 13.0 (SPSS, Chicago, IL). The level of statistical significance was set at $p \leq 0.05$.

### Table 3  Mean values and standard deviation of number of loading cycles

<table>
<thead>
<tr>
<th>Group defined for stepping rate (bpm)</th>
<th>n</th>
<th>Osteogenic index</th>
<th>GRF (in BW)</th>
<th>Loading cycles</th>
<th>Duration (min)</th>
</tr>
</thead>
<tbody>
<tr>
<td>(1) 124.1–130 bpm</td>
<td>26</td>
<td>11.65 ± 0.87</td>
<td>1.39 ± 0.09</td>
<td>4362.9 ± 1020.3</td>
<td>43.2 ± 7.6</td>
</tr>
<tr>
<td>(2) 130.1–135 bpm</td>
<td>32</td>
<td>11.76 ± 0.73</td>
<td>1.42 ± 0.08</td>
<td>4031.3 ± 1022.6</td>
<td>36.9 ± 8.3</td>
</tr>
<tr>
<td>(3) 135.1–140 bpm</td>
<td>37</td>
<td>12.31 ± 0.76</td>
<td>1.48 ± 0.09</td>
<td>4174.8 ± 1016.9</td>
<td>37.0 ± 7.4</td>
</tr>
<tr>
<td>(4) 140.1–144.7 bpm</td>
<td>5</td>
<td>12.08 ± 0.88</td>
<td>1.44 ± 0.09</td>
<td>4501.4 ± 1720.6</td>
<td>37.0 ± 11.5</td>
</tr>
</tbody>
</table>

Maximal vertical ground reaction forces (GRF) in normalised body weight (BW), osteogenic index, and duration for the four groups defined by stepping rate.
RESULTS

Table 2 indicates that the mean (+SD) number of loading cycles was 4194.1 ± 1055.2 (range 1874–7250), the mean (+SD) number of movements was 1422.6 ± 384.5 (range 624–2524), the mean (+SD) percentage of non-propulsion movements was 79.4 ± 10.5% (range 48–100%), and the mean (+SD) percentage of propulsion movements was 20.6 ± 10.5% (range 0–52%). Step movements and frequency performed are presented in fig 1. Marching was the exercise performed most often in the 100 sessions (29,575 times); the four step movements performed most often were knee hop (variant of knee lift with propulsion), side leg (variant of knee lift), L step (variant of knee lift), and over the top (variant of basic step) which were performed 8432, 8154, 7638, and 6972 times, respectively.

Interestingly, the majority of participants were female. In all classes most of the participants used a 15 cm high bench and hand weights were not used. Mean (+SD) magnitude of peak vertical GRF was 1.40 ± 0.10 BW (range 1.26–1.65), according to the motor patterns performed, and mean (+SD) osteogenic index was 12.0 ± 0.8 (10.3–14.0).

For better analysis in practical terms, step sessions were divided into four groups according to stepping rate as follows: (1) 124.1–130 bpm; (2) 130.1–135 bpm; (3) 135.1–140 bpm; and (4) 140.1–144.7 bpm. Mean values (+SD) of number of loading cycles, maximal vertical GRF, osteogenic index, and duration for these four groups are presented in table 3.

A one way ANOVA was conducted with a Tukey post hoc test for each variable in order to compare them among these groups.

The mean osteogenic index was compared among these groups (fig 2). Osteogenic index increases significantly when stepping rate is higher than 135 bpm, being significantly different among the stepping rate groups (F(3,36) = 8.132; p = 0.000). These differences were found between the 124.1–130 bpm and 135.1–140 bpm groups (p = 0.001), and between the 130.1–135 bpm and 135.1–140 bpm groups (p = 0.001).

Mean peak vertical GRF in BW was compared among these groups (fig 3). Peak GRF increases significantly when stepping rate is higher than 135 bpm, being significantly different among stepping rate groups (F(3,36) = 10.727; p = 0.000). Post hoc tests indicated that these differences were found between the 124.1–130 bpm and 135.1–140 bpm groups (p = 0.001), and between the 130.1–135 bpm and 135.1–140 bpm groups (p = 0.000).

The mean number of loading cycles per session was compared among these groups (fig 4). The number of loading cycles was higher in the two groups with faster cadence. However, no significant differences were found among groups regarding the number of loading cycles (F(3,36) = 0.574; p = 0.633). Mean session duration was similar among groups with no significant differences between them (F(3,36) = 0.836; p = 0.477).

For better analysis in practical terms, step sessions were divided into groups according to duration as follows: (1) 25–30 min; (2) 30.1–35 min; (3) 35.1–40 min; (4) 40.1–45 min; and (5) 45.1–58 min. Mean values and standard deviation of...
Stepping rate was similar among session duration groups (F(4,95) = 2.011; p = 0.099) on the dependent variable stepping rate. Stepping rate was similar among the five groups (fig 5), being significantly different among the session duration groups (F(4,95) = 3.616; p = 0.009). These differences were found between the 30.1–35 min and 35.1–40 min groups (p = 0.036), and between the 30.1–35 min and 45.1–58 min groups (p = 0.024).

The mean peak vertical GRF in BW was compared among these groups (fig 6). There was a significant difference among session duration groups (F(4,95) = 4.105; p = 0.004) on the dependent variable GRF. These differences were found between the 25–30 min and 30.1–35 min groups (p = 0.036), and between the 25–30 min and 40.1–45 min groups (p = 0.012).

The mean number of loading cycles per session was compared among these groups (fig 7). There was a significant difference among session duration groups (F(4,95) = 26.872; p = 0.000) on the dependent variable number of loading cycles, which increases progressively, as would be expected. These differences were found between the 25–30 min and 30.1–35 min groups (p = 0.044), between the 25–30 min and 35.1–40 min groups (p = 0.000), between the 25–30 min and 40.1–45 min groups (p = 0.000), between the 25–30 min and 45.1–58 min groups (p = 0.000), between the 30.1–35 min and 40.1–45 min groups (p = 0.001), between the 30.1–35 min and 45.1–58 min groups (p = 0.000), and between 35.1–40 min and 45.1–58 min groups (p = 0.001).

A one way ANOVA was conducted with a Tukey post hoc test in order to compare variables among these groups.

The mean osteogenic index was compared among these groups (fig 5), being significantly different among the session duration groups (F(4,95) = 3.616; p = 0.009). These differences were found between the 30.1–35 min and 35.1–40 min groups (p = 0.036), and between the 30.1–35 min and 45.1–58 min groups (p = 0.024).

The mean number of loading cycles per session was compared among these groups (fig 7). There was a significant difference among session duration groups (F(4,95) = 26.872; p = 0.000) on the dependent variable number of loading cycles, which increases progressively, as would be expected. These differences were found between the 25–30 min and 30.1–35 min groups (p = 0.044), between the 25–30 min and 35.1–40 min groups (p = 0.000), between the 25–30 min and 40.1–45 min groups (p = 0.000), between the 25–30 min and 45.1–58 min groups (p = 0.000), between the 30.1–35 min and 40.1–45 min groups (p = 0.001), between the 30.1–35 min and 45.1–58 min groups (p = 0.000), and between 35.1–40 min and 45.1–58 min groups (p = 0.001).

The mean stepping rate was compared among these groups. There was no significant difference among the five session duration groups (F(4,95) = 2.011; p = 0.099) on the dependent variable stepping rate. Stepping rate was similar among groups.

Osteogenic index, maximal vertical GRF in normalised BW weight, number of loading cycles, stepping rate for these five groups are presented in table 4.

<table>
<thead>
<tr>
<th>Groups defined for duration (min)</th>
<th>n</th>
<th>Osteogenic index</th>
<th>GRF (in BW)</th>
<th>Loading cycles</th>
<th>Stepping rate (bpm)</th>
</tr>
</thead>
<tbody>
<tr>
<td>(1) 25–30 min</td>
<td>23</td>
<td>11.88 ± 0.61</td>
<td>1.48 ± 0.07</td>
<td>3516 ± 760.8</td>
<td>136.0 ± 4.5</td>
</tr>
<tr>
<td>(2) 30.1–35 min</td>
<td>22</td>
<td>11.58 ± 0.62</td>
<td>1.41 ± 0.07</td>
<td>3774 ± 445.1</td>
<td>135.3 ± 3.7</td>
</tr>
<tr>
<td>(3) 35.1–40 min</td>
<td>20</td>
<td>12.28 ± 0.96</td>
<td>1.47 ± 0.10</td>
<td>4355 ± 824.3</td>
<td>135.2 ± 4.9</td>
</tr>
<tr>
<td>(4) 40.1–45 min</td>
<td>17</td>
<td>11.73 ± 0.89</td>
<td>1.39 ± 0.10</td>
<td>4727 ± 839.3</td>
<td>132.6 ± 5.5</td>
</tr>
<tr>
<td>(5) 45.1–58 min</td>
<td>18</td>
<td>12.34 ± 0.84</td>
<td>1.44 ± 0.09</td>
<td>5355 ± 791.1</td>
<td>133.2 ± 4.5</td>
</tr>
</tbody>
</table>

Values are mean ± SD. BW, body weight.

DISCUSSION

This may be the first study to characterise step exercise sessions as they really happen in practice, and to calculate the osteogenic index. Step exercise is far from being defined by basic steps at 122 bpm as initially proposed by its creators. The mean and standard deviation values for stepping rate were 134.6 ± 4.7 bpm, ranging from 120 to 130 bpm, which means that cadence varied from slow to fast. Step sessions have many different easy and complex movement patterns. Thirty seven different movement patterns were identified, which produce different biomechanical loads. Most of the participants used step benches 15 cm high, as expected. However, as discussed in a previous study,2 a 10 cm step bench might be more appropriate depending on age, expertise level, and choreography (for example, for the elderly, beginners, very young people, pregnant women, and those with previous knee injury or undergoing rehabilitation). The three main determinants of exercise intensity that can be manipulated by instructors are bench height, stepping rate, and choreography. Thus, further research concerning these variables is essential.

The mean(± SD) weighted peak ground reaction force normalised to body weight was 1.4 ± 0.1 BW, ranging from 1.26 to 1.65 BW, according to the motor patterns performed. Based upon the literature and preliminary laboratory studies, high skeletal loading intensity has been defined as GRF of greater than 4 BW, moderate intensity as 2–4 BW, and low intensity as less than 2 BW. 15 16 However, further research is needed concerning the GRF of different step movements performed at different cadences. Nevertheless, the result of the loading on the body depends on three factors: the magnitude of the force, the rate at which the force is applied, and the repetition of load application.20

Stepping rate is one determinant of mechanical intensity. OI and GRF increase significantly when stepping rate is
higher than 135 bpm. This stepping rate might be used as a reference for higher intensity classes. Also, OI, GRF, and loading cycles are higher in classes where cadence is faster. Session duration also seems to have an influence on these variables, especially the number of loading cycles, as expected, but seems to have no influence on stepping rate, which means that a 30 min workout using fast cadences might induce similar amounts of loading as longer sessions.

According to Turner and Robling, if the osteogenic response to exercise is enhanced by regimens that incorporate periods of rest between short vigorous skeletal loading sessions, a frequency of two to three sessions per week of step exercise is sufficient. Despite the benefits claimed for step classes correctly structured and adapted to participants, further research is needed regarding exercise prescription and injury prevention. Additional study is also required concerning the biomechanical load of this activity, as there is no information concerning GRF for many of the stepping patterns and stepping rates.

The OI can also be used to compare different physical activities. Using the same calculations, a simulation was done for one, three, and five sessions of walking and stepping per week, as presented in fig 8. The example given by Turner and Robling was used for walking. As shown in the figure, step exercise has a higher OI than walking, meaning that stepping exercise of the same intensity (duration and frequency) as walking might be more effective in terms of OI. Other exercises could be compared when there is more information on their physical activity characteristics (number of loading cycles) and biomechanical loading (GRF).

The present study should be replicated in the future, when more information becomes available concerning the GRF of different movement patterns and stepping rates. Also, a worksheet might be developed in order to quickly estimate the osteogenic potential of exercise.

CONCLUSIONS
The Turner and Robling osteogenic index might be useful for better understanding of the positive association between exercise and bone health. OI depends on the GRF of activities which in turn depend on the types of movements and stepping rate. The mean (± SD) osteogenic index of 100 step classes was 12.0 ± 0.8 (range 10.3–14.0), the stepping rate was 134.6 ± 4.7 bpm (120–150 bpm), and the total number of loading cycles was 4194.1 ± 1055.2 (which might help to meet the recommended 10 000 steps a day). OI and GRF increase significantly when stepping rate is higher than 135 bpm. In practical terms, step exercise seems to provide a healthy mechanical stimulus, if safely performed, with mechanical load falling between that provided by walking and running. Stepping rate is a very important determinant of mechanical intensity and should be carefully chosen by instructors according to the participants’ level of expertise.

Figure 8  Osteogenic index calculated for step exercise and walking depending on session duration (in minutes) and frequency (number of sessions per week).

What is already known on this topic
- Step exercise is a low impact physical activity recommended for the improvement of cardiorespiratory and muscular fitness
- The mechanical loads experienced during step exercise may improve bone health
- A measure of the effectiveness of exercise protocols is provided by the osteogenic index which estimates bone formation according to exercise intensity and desensitisation

What this study adds
- A hundred step exercise sessions have been characterised and their osteogenic index calculated
- Differences were found in osteogenic index depending on session duration and stepping rate
- The osteogenic indices of step and walking exercises have been compared.
Despite the stated benefits when step classes are correctly structured and adapted to the participants’ level of expertise, further research is needed concerning biomechanical loading to improve exercise prescription and prevent injury.

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There are no competing interests.

REFERENCES

This paper provides data on and analyses of the moderators of step exercise and their relationship to the osteogenic index, which depends on peak ground reaction force. Comparisons with walking and running are made and data from fundamental research studies highlighting the relative values of alternative exercise regimes are presented. Such information can aid in the provision of more accurate and varied exercise prescription and the design of training programmes in sport and rehabilitation.